



Title: Muscle deoxygenation during moderate- and severe-intensity cycling in youth elite-cyclists

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Keywords: muscle oxygenation, oxidative metabolism, adolescent cyclists, reliability

Background: Near-infrared spectroscopy (NIRS) is a well-established technique to measure tissue oxygenation and haemodynamics during exercise. While muscle oxygen consumption is derived by measuring concentration changes of oxygenated and deoxygenated haemoglobin and myoglobin (O₂Hb and HHb), total haemoglobin (tHb = O₂Hb + HHb) reflect blood volume and perfusion. In particular, the change in HHb is considered a proxy for oxygen extraction at the muscle level during exercise and arterial occlusion, where the rate of reoxygenation has been used as a measure of mitochondrial function (Ryan et al, 2012: Journal of Applied Physiology, 113, 175-183). NIRS-derived signals therefore reflect the dynamic balance between oxygen delivery and utilisation and may be important measures to monitor training induced adaptations of aerobic function in skeletal muscle. However, current literature is scarce regarding reliability measures, especially in young athletes, which needs to be established to interpret changes with confidence.

Purpose: To assess the test-retest reliability of HHb-changes during moderate- and severe-intensity cycling, and during arterial occlusion in youth elite-cyclists.

Methods: Fifteen cyclist (mean \pm SD: age 13.5 ± 1.8 y; stature 163.2 ± 12.2 cm; body mass 51.3 ± 12.4 kg; $\dot{V}O_{2\max}$ 62.1 ± 4.2 mL \cdot min⁻¹ \cdot kg⁻¹) completed two 6-min rest-to-work transitions (T) from baseline (BL: 60 W) to moderate- (90% of the first ventilatory threshold [VT1]: 120 ± 26 W) and to severe- (50% between VT and maximum power [Delta50]: 204 ± 43 W) intensity cycling. The transitions were interspersed by 8 min BL cycling. After Delta50 cycling, an occlusion was applied on the proximal thigh at a pressure of 300 mmHG until a levelling-off of the HHb signal was observed (3-5 min). The protocol was repeated after a passive rest of 1 h. Changes in HHb were measured on the belly of the right vastus lateralis muscle with a portable continuous-wave NIRS device at a sampling rate of 5 Hz (PortaMon, Artinis). Second-per-second data, were corrected for blood volume changes and normalised to the full functional range measured during the occlusion (0-100%). HHb changes (%) were calculated from BL to the maximum of VT1 (Δ BL-VT1) and from BL to the maximum of Delta50 (Δ BL-Delta50). In addition, the reoxygenation after occlusion was assessed with the slope of linear regression analysis (% \cdot s⁻¹). A typical example of the HHb signal is shown in Figure 1. Absolute and relative reliability was calculated with Bland-Altman statistics \pm 95% limits of agreement and the coefficient of variation (CV; %), respectively. Paired t-tests were used for comparisons.



Results: The $\Delta\text{BL-VT1}$ was 20.5 ± 11.7 and $21.6 \pm 12.3\%$ during T1 and T2, respectively ($p = 0.079$). The bias was $1.1 \pm 2.3\%$ (95% LoA: $-5.6 - 3.3$) and the CV 10.1% ($7.3 - 16.4$). The $\Delta\text{BL-Delta50}$ were 58.1 ± 9.6 (T1) and $56.5 \pm 9.3\%$ (T2) ($p = 0.133$) and the bias and CV were $1.6 \pm 3.9\%$ ($-6.0 - 9.3$) and 5.4% ($3.9 - 8.6$), respectively. The reoxygenation slopes were 7.2 ± 2.0 (T1) and $7.6 \pm 2.1\% \cdot \text{s}^{-1}$ (T2) ($p = 0.053$) with a bias and CV of $0.4 \pm 0.7\% \cdot \text{s}^{-1}$ ($-1.8 - 1.0$) and 7.0% ($5.1 - 11.2$), respectively.

Discussion: The present study quantified reliability for NIRS-derived changes in HHb during cycling at moderate and severe intensity as well as for reoxygenation after occlusion. The provided levels of 5.4% for severe-intensity cycling and 7.0% for the reoxygenation slope, are well below the level of 10% considered as acceptable for a measurement, and the level of 10.1% for moderate-intensity cycling is only marginally higher. The reliability data established, provide limits within which training induced adaptations may be interpreted with confidence. Longitudinal studies in young athletes could potentially benefit from these findings since the magnitude of changes in NIRS variables is probably greater than the reported measurement error.

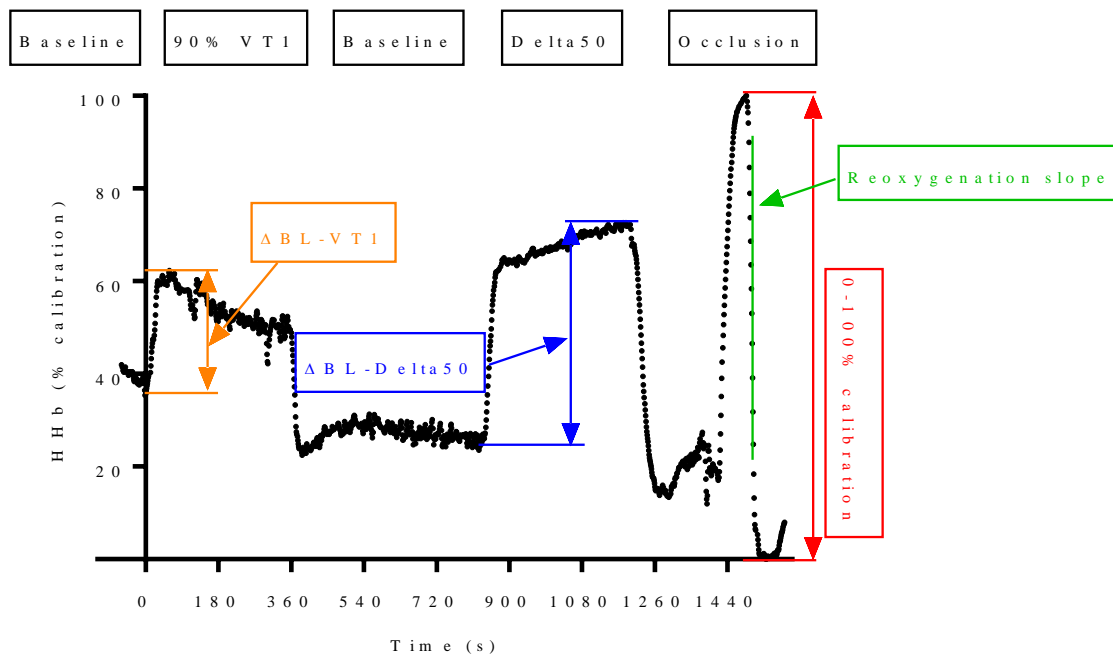


Figure 1: Typical pattern of the HHb response from a representative subject. During moderate cycling HHb increased within 60 s from BL to VT1-maximum and subsequently decreased until end-exercise, indicating an increase in muscle perfusion. During severe cycling the HHb showed a continuous increase until end-exercise.